



MASSACHUSETTS  
GENERAL HOSPITAL

# Comparison of Diffusion and Transport in Human Head

Comparison of Monte Carlo and Finite Difference predictions of  
near-infrared light propagation in realistic adult head model

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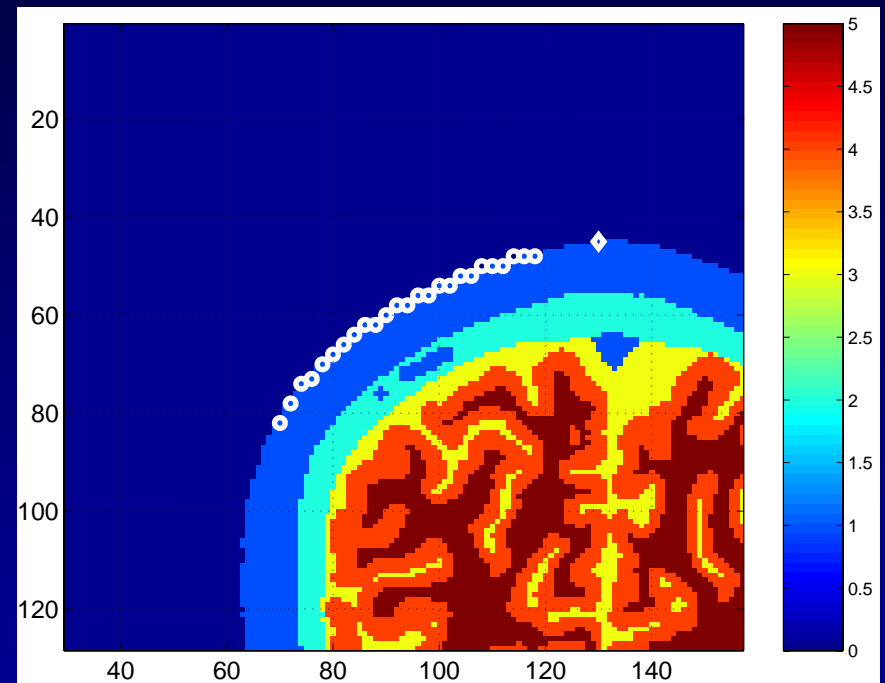
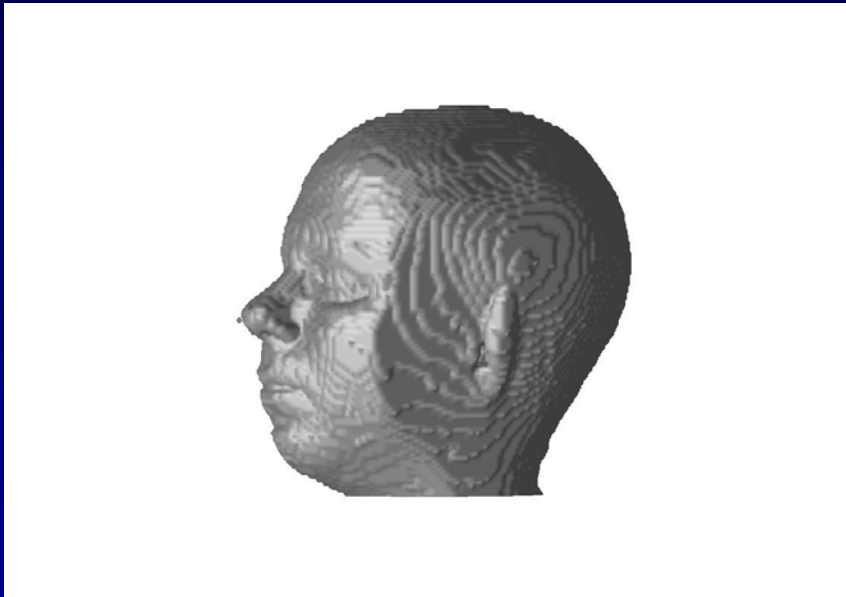
# Outline

- Overview of the problem and framework
- Two (related) questions:
  - Monte Carlo (MC) or Finite Difference (FD)?
  - Cerebral Spinal Fluid (CSF) optical properties? CSF modelling?
- Our model:
  - Head geometry and probe
  - Tests and setup
  - Results
  - Starting the inverse problem...
- Conclusions
- Future work

# Diffuse Optical Tomography (DOT)

- Biological tissue imaging: brain and breast
- Brain
  - Baseline
  - activation: why?
- Head geometry: MRI structural data...
  - Optical properties (5): absorption coefficient ( $\mu_a$ ) and scattering coefficient ( $\mu_s$ )
  - Probe and opdots structure

# Adult head geometry



# Monte Carlo (MC)

- Based on Transport equation
- Pro
  - accuracy
  - robustness
- Cons
  - Computational cost
  - Low Signal to Noise Ratio (SNR)

# Finite Difference (FD)

- Based on Diffusion Approximation (DA)
- Cons: limited by
  - Boundary Conditions (BC)
  - rough surface
  - small scattering
- Pro
  - Computational cost
  - Good Signal to Noise Ratio (SNR)

# Monte Carlo (MC) vs. Finite Difference (FD)

- When can we rely on the faster FD?  
[CSF]
- How much can we rely on FD?  
[qualitative-quantitative tests]
- How can we improve FD response?  
[finer lattice plus zero-padded head]
- How much does MC-FD discrepancy affect the optical properties restoration?  
[inverse problem exploration]

# Brain activation overview

- Brain activity: BOLD, CBF, CBV, Hbr and HbO

$$(1 + rCMRO_2) = (1 + rCBF)(1 + rCBV_{ven})^{-1}(1 + rHbr_{ven})$$

- Measuring Hemodynamic: hemoglobin concentration

$$SO_2 = \frac{[HbO_2]}{[HbO_2 + Hbr]}$$

$$\begin{cases} \mu_{a,780} = c[Hbr] \cdot \epsilon_{[Hbr],780} + c[HbO_2] \cdot \epsilon_{[HbO_2],780} \\ \mu_{a,830} = c[Hbr] \cdot \epsilon_{[Hbr],830} + c[HbO_2] \cdot \epsilon_{[HbO_2],830} \end{cases}$$



# Tests overview

- Frequency = 0
- Continuous Waves (CW) and Time Domain (TD)
- MC SNR: combination of 11 runs (x100 million photons)
- Linear probe (1 source, 25 detectors)
- Optical properties:

Tissue type	Absorption coefficient ( $\text{mm}^{-1}$ )	Scattering coefficient ( $\text{mm}^{-1}$ )
Scalp and Skull	0.019	0.86
CSF	0.004	1.0, 0.7, 0.1, 0.2, 0.3, 0.01, 0.001
Gray and White matter	0.01	1.11

# Tests overview

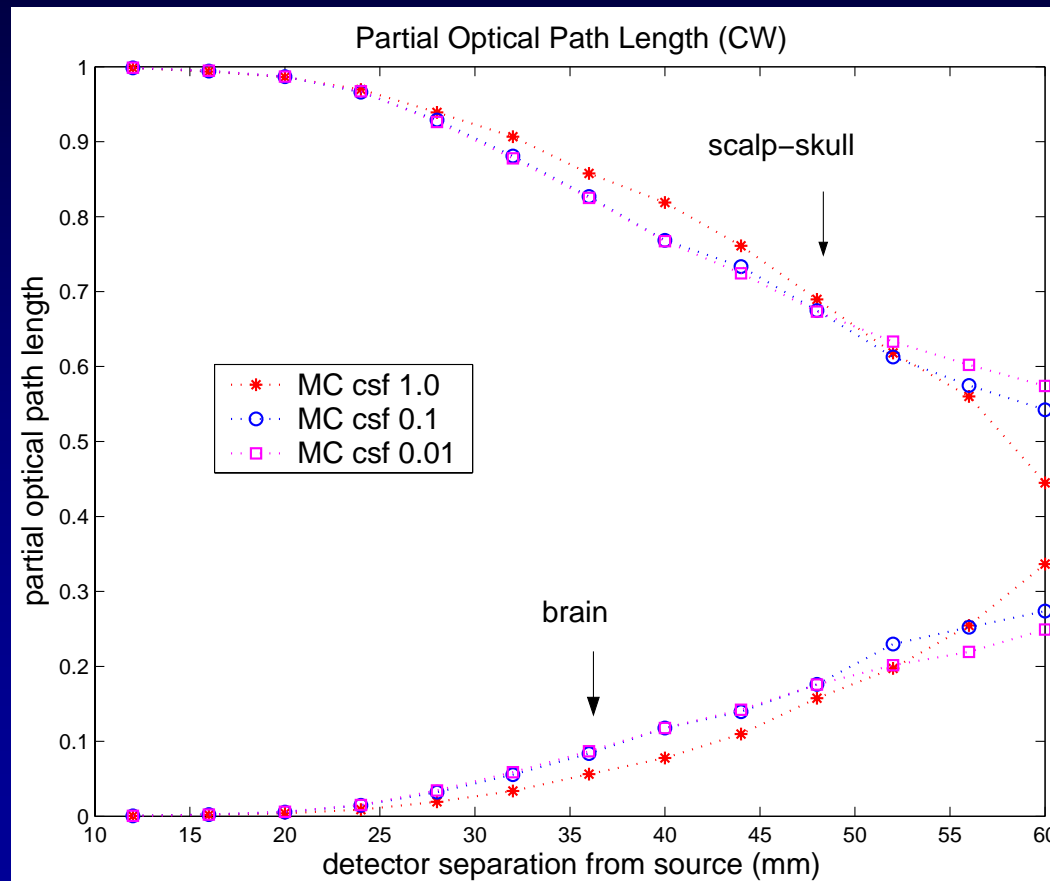
- TPSF: Temporal Point Spread Function
- PPF: Partial Optical Path Length Factor

$$\frac{\partial f(t)}{\partial \mu_{a_i}} = \frac{(f_{\mu_{a_0}}(t) - f_{\mu_{a_i}}(t))}{\Delta \mu_a}$$

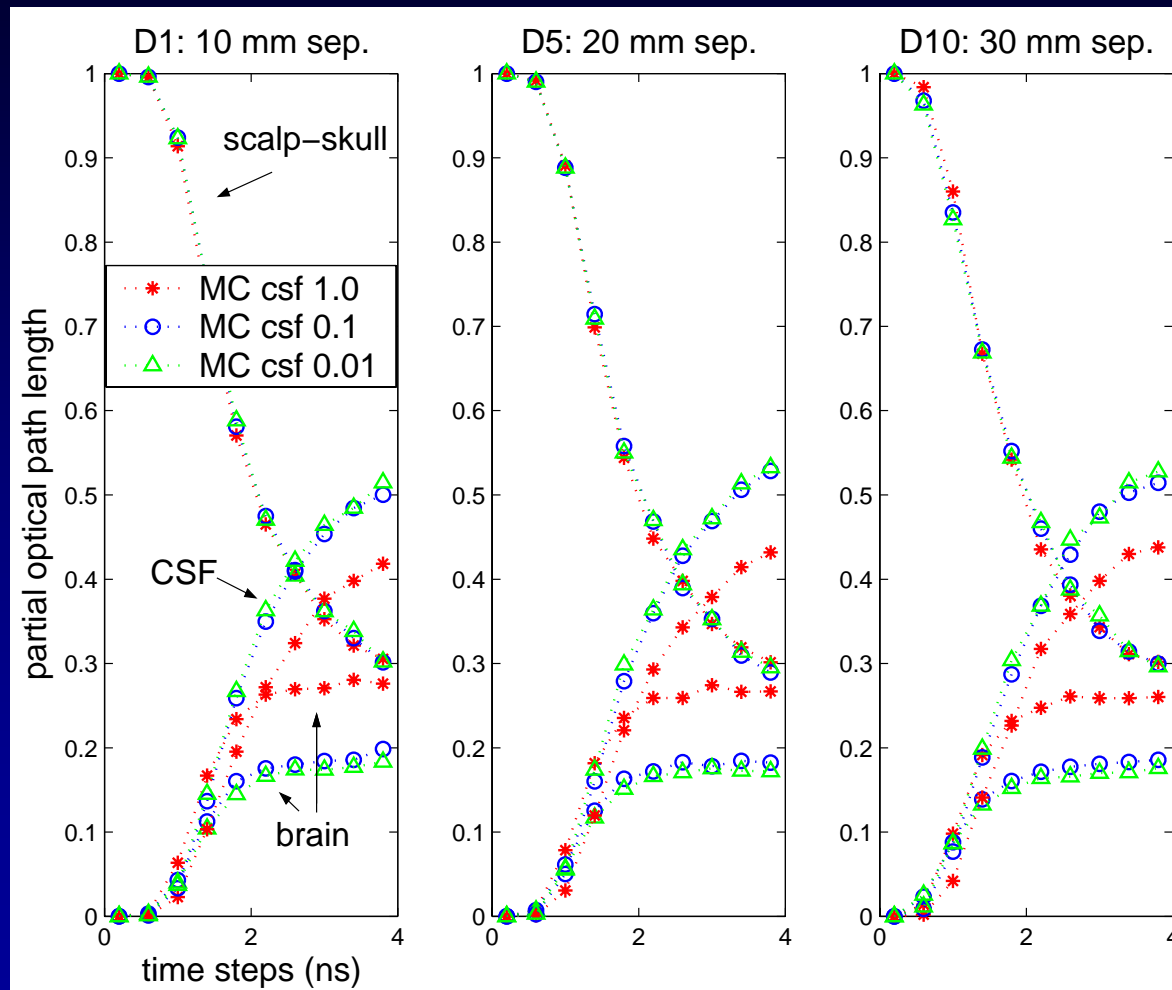
- CW: Continuous Wave (spatial sensitivity profile)
- Test structure
  - Pre-tests on MC
  - Pre-tests on FD finer lattice
  - Tests on MC v. FD

# Pre-tests: CSF [CW]

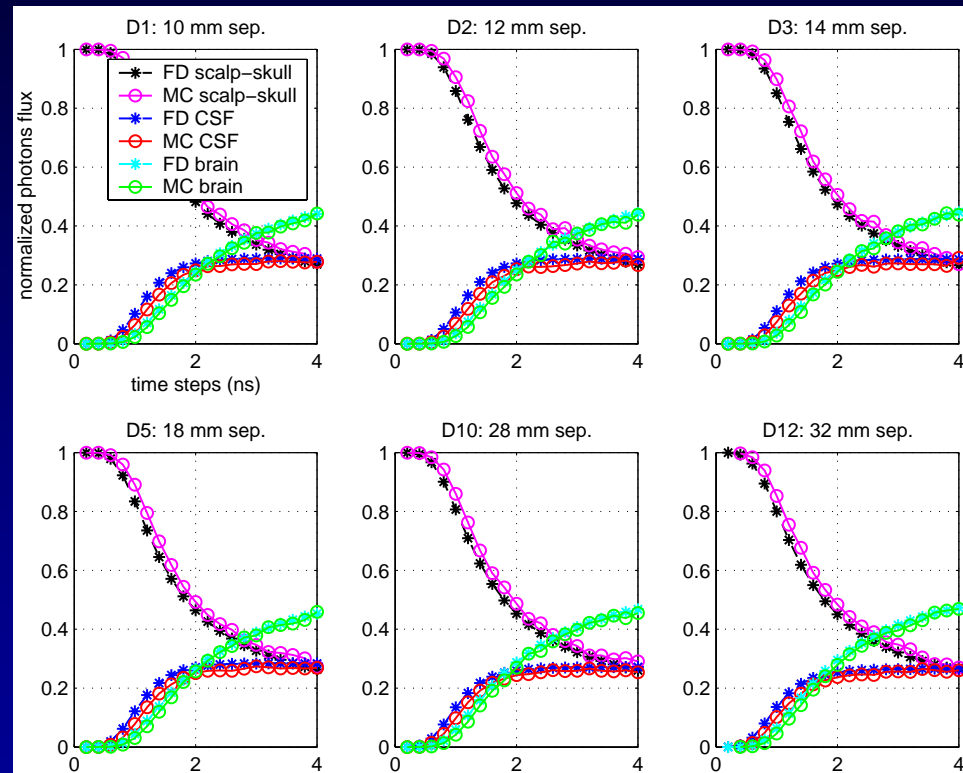
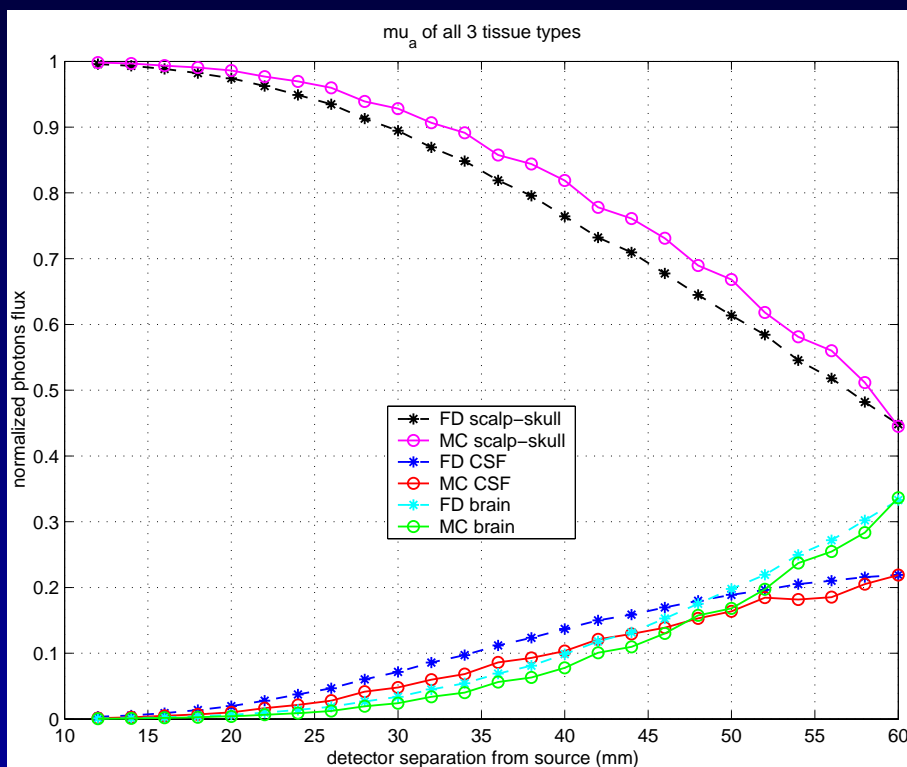
CSF scattering coefficient estimation (via MC CW and TD simulations)



# Pre-tests : CSF [TD]

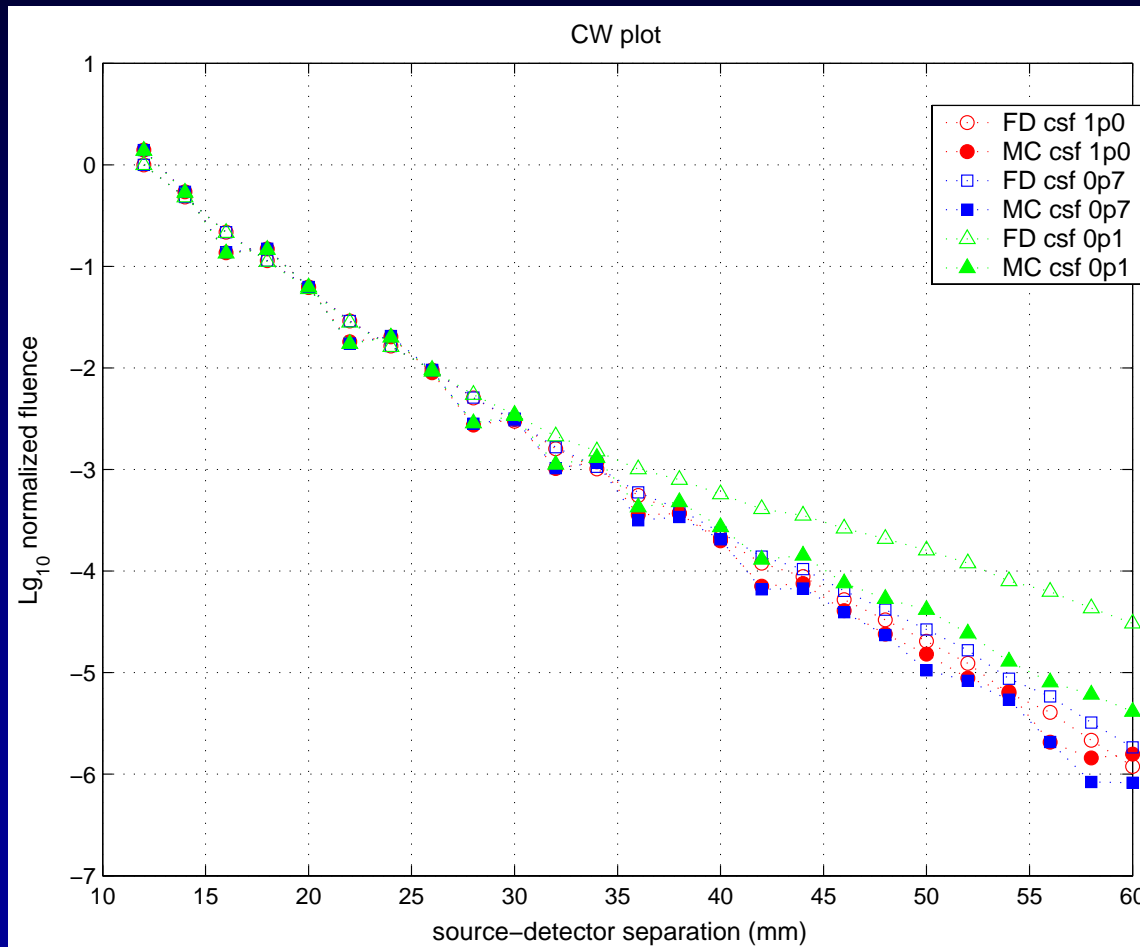


# Pre-tests: finer lattice

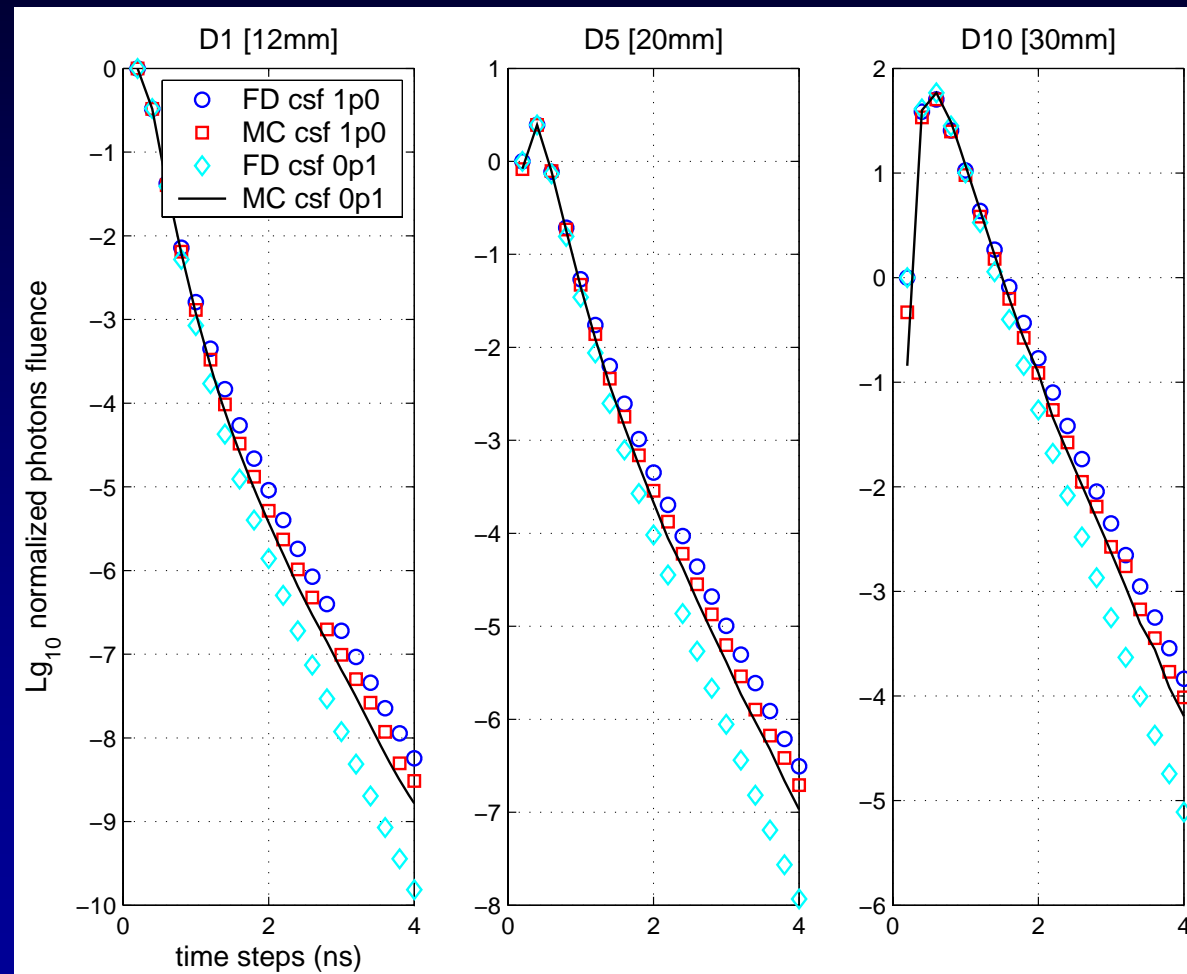


FD  $dx$  2 mm;  $\mu_{s,CSF}$  1.0 mm<sup>-1</sup>

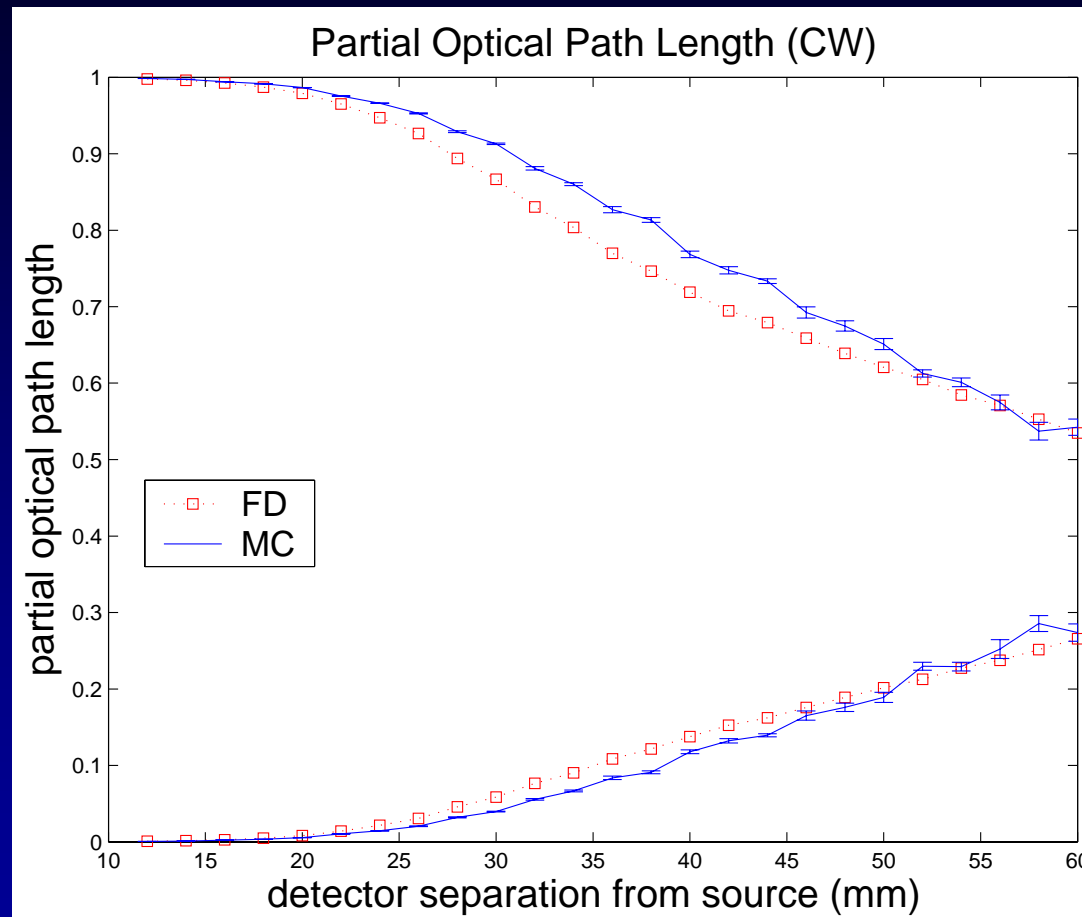
# Results: Spatial Sensitivity Profile



# Results: TPSF



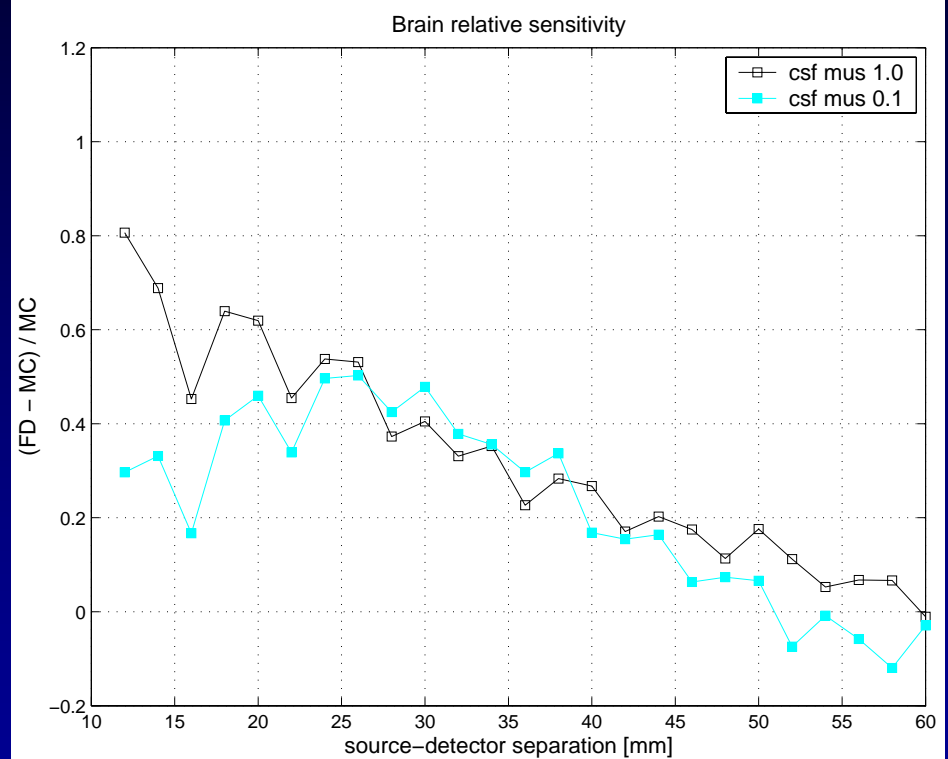
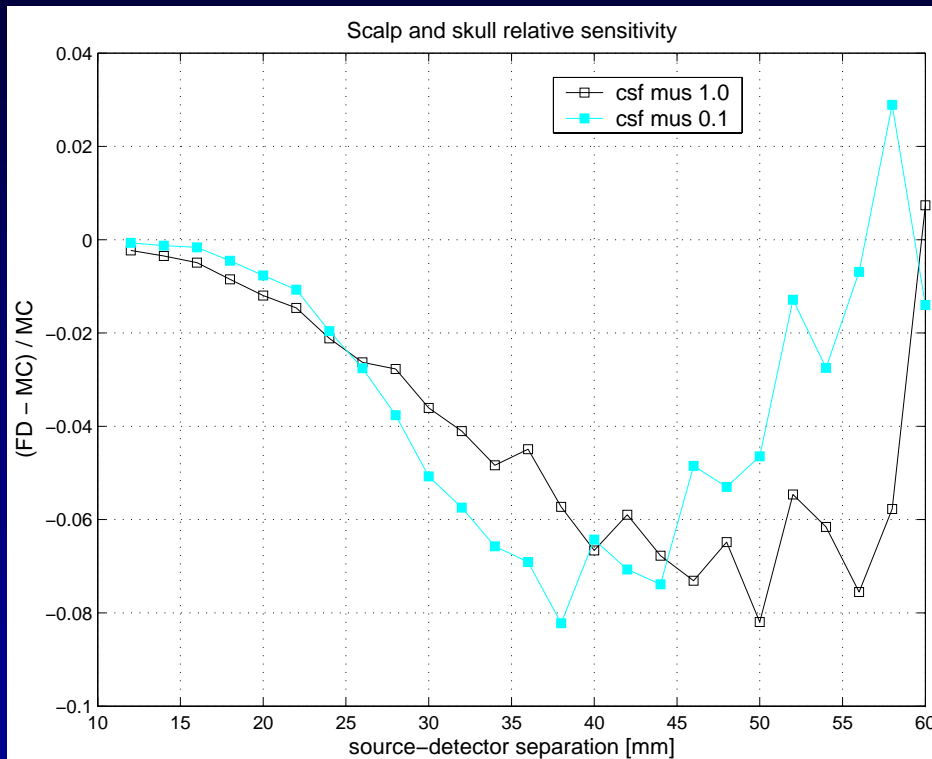
# Results: Partial Optical Path-Length



PPF MC v. FD (dx 1 mm) [CW  $\mu_{s,CSF}$  0.1 mm<sup>-1</sup>]

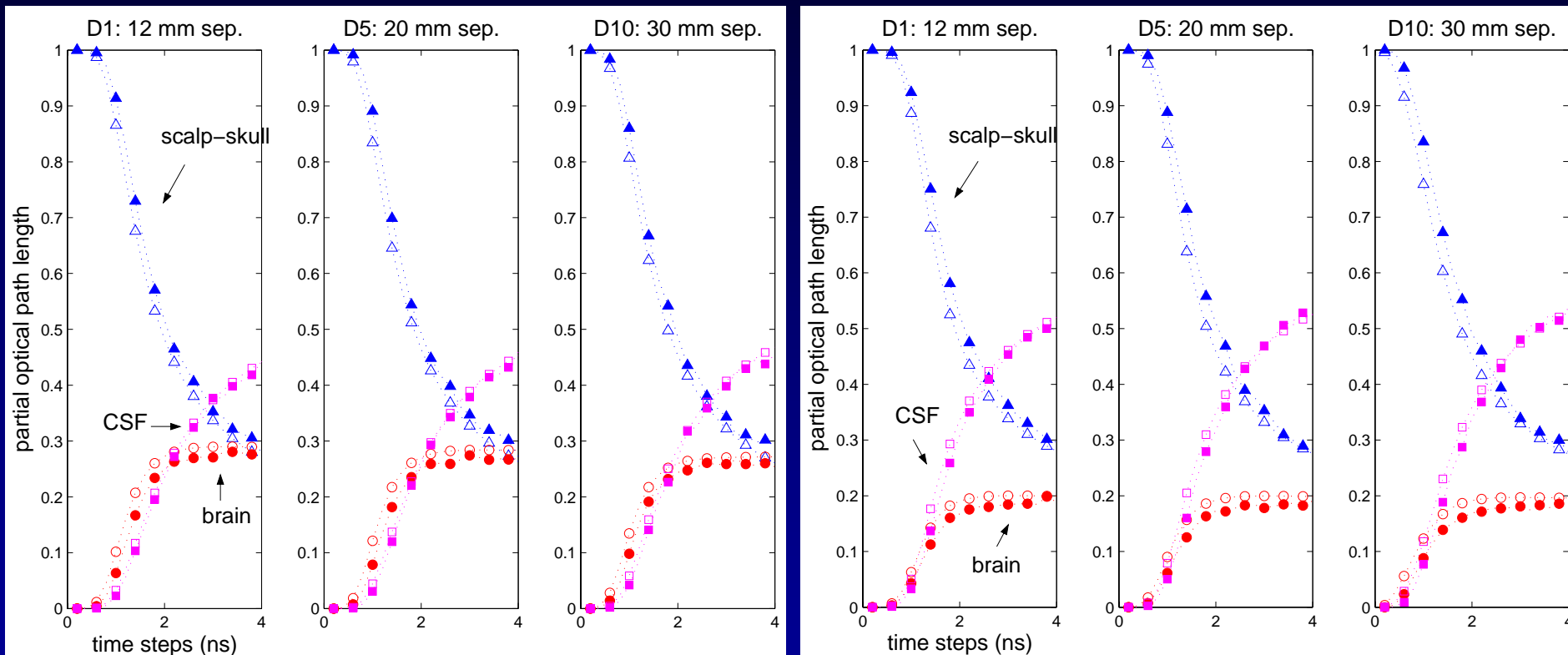


# Results: Partial Optical Path-Length



PPF MC and FD relative discrepancy [CW]  
[w.r.t. MC]

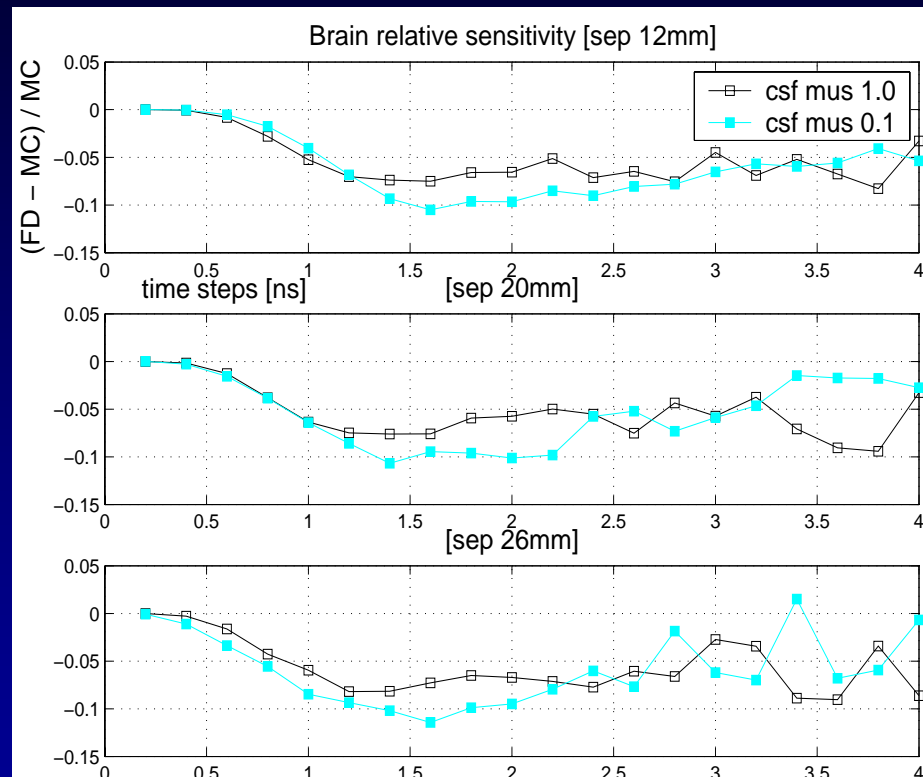
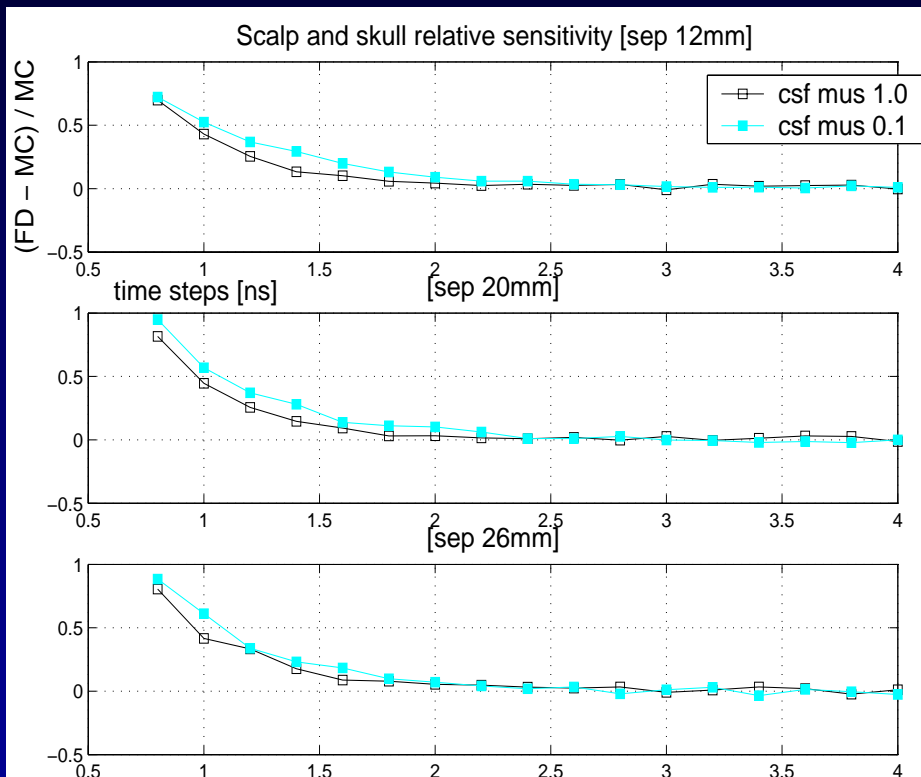
# Results: Partial Optical Path-Length



PPF MC v. FD (dx 1 mm) [TD]

[right  $\mu_s, \text{CSF} 1.0 \text{ mm}^{-1}$ ; left  $\mu_s, \text{CSF} 0.1 \text{ mm}^{-1}$ ](full MC, empty FD)

# Results: Partial Optical Path-Length



PPF MC and FD relative discrepancy [TD]  
[w.r.t. MC]

# Conclusions

- FD reliable for “reasonable” optical properties:
  - CSF: good characterization
  - Accurate head model
  - Finer lattice improves FD reliability but increases run time (zero-padding)

# Future work

- Forward model:
  - BC for FD
  - Finer lattice (smoother edges)
  - Use all 5 tissue types
  - Combine multiple sources
  - Use multiple wavelengths
- Inverse model:
  - Tune optimal parameters and stopping criteria
  - Regularization parameters
  - Linear and Non-linear approaches
  - Comparing various inverse techniques

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Thank you!



...Questions?

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